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APPARATUS FOR FACILITATING
TRANSDERMAL DELIVERY OF THERAPEUTIC SUBSTANCES AND METHOD
OF TRANSDERMALLY DELIVERING THERAPEUTIC SUBSTANCES

5 Field of the Invention

The present invention relates to an apparatus for facilitating transdermal delivery of therapeutic substances and to a method of transdermally delivering therapeutic substances.

Background of the Invention

The use of therapeutic substances to treat and/or prevent disease, injury or disability is a cornerstone of modern human and animal related medicine.

In order for such therapeutic substances to have useful effect to a desired treatment area, the substances must be physically and/or chemically available to the treatment area, and must be available in a sufficient concentration to exert a beneficial biological effect.

As an alternative to conventional methods of delivery of therapeutic substances, transdermal delivery techniques have been developed so that a degree of site specificity is obtained and a desired concentration of therapeutic substance is achieved which is unaltered by digestion or blood chemistry. Transdermal delivery techniques also offer the possibility of high user compliance, ease of management, low toxicity and high cost effectiveness.

However, mammalian skin poses a significant barrier to entry for many therapeutic substances because the lipid bilayer of the stratum corneum skin layer generally only allows very small neutrally charged particles of the order of 1nm to pass through. As such, transdermal delivery of

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many ions, drugs, macro molecules, DNA fragments, genes and therapeutic substances is problematic.

5 In one transdermal technique referred to as iontophoresis, an electrical energy gradient is used to charge a target molecule and an electrical voltage is employed to accelerate the charged target molecule towards a cell membrane adjacent the target area, the energy of the target molecule being sufficient to cause the target
10 molecule to pass through the cell membrane.

However, due to the relatively high energy levels employed, significant residual cellular damage occurs to the skin which can manifest as localised burns, skin
15 irritation and cellular fatigue. In addition, critical ionic structures of the target molecule can be inadvertently changed by the process.

A further transdermal delivery technique is referred to as
20 electroporation. With this technique, successive pulses of 1ms to 10ms duration of the order of 100 to 200 volts are directly applied to a target skin area using probes.

However, as with the iontophoresis technique, since
25 relatively high energy levels are used, significant cellular damage occurs. In addition, in view of the high voltages employed, electroporation is unsuitable to use in vivo and to date has been used only in vitro.

30 The barrier effect of the stratum corneum arises as a result of the intercellular lipid matrix which comprises long chain ceramides, free fatty acids, cholesterol and other lipids. The lipids are arranged into bilayers having hydrocarbon chains aligned to form an oily bilayer
35 core and electrically charged or polar outwardly facing head groups. This produces a highly selective filter-like structure. In contrast to phospholipid bilayer membranes

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found elsewhere in the body, the composition of the stratum corneum lipid bilayers is a much more rigid and ordered structure. As a consequence, the barrier to penetration of the stratum corneum by therapeutic
5 substances is much greater compared to the corresponding barriers to penetration produced by other body membranes.

Therapeutic substance delivery techniques such as iontophoresis and electroporation rely on introducing
10 sufficient energy to the stratum corneum to break up the inherent structure of the lipid bilayer, which disrupts the hydrophilic-hydrophobic orientation of the bilayer and creates regions of random orientation through which some substances may be introduced. Disruption of the dermal
15 barrier effect in this way is unpredictable and provides little control over the rate of drug delivery.

In the claims of this application and in the description of the invention, except where the context requires
20 otherwise due to express language or necessary implication, the words "comprise" or variations such as "comprises" or "comprising" are used in an inclusive sense, i.e. to specify the presence of the stated features but not to preclude the presence or addition of further
25 features in various embodiments of the invention.

Summary of the Invention

In accordance with an aspect of the present invention,
30 there is provided an apparatus for facilitating transdermal delivery of therapeutic substances, said apparatus comprising:

 means for producing an electromagnetic field;
 control means arranged to control said field
35 producing means to alternately produce active and substantially inactive electromagnetic field portions, each said active electromagnetic field portion including

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an electromagnetic field packet having a plurality of successive electromagnetic field pulses, and each said substantially inactive electromagnetic field portion including no electromagnetic field pulses;

- 5 wherein during use when the electromagnetic field is incident on a patient, dermal permeability is increased.

In one arrangement, the means for producing an electromagnetic field includes a coil. The means for
10 producing an electromagnetic field may further include a solid state switching device which may be a transistor such as a bipolar transistor connected in series with the coil.

- 15 In one arrangement, the control means is arranged to produce an energisation signal useable to control switching of the solid state switching device, the energisation signal including a repeating energisation signal packet, each energisation signal packet including a
20 plurality of energisation signal pulses of generally rectangular configuration.

The control means may comprise a microcontroller which may be programmable by a user. The microcontroller may be
25 programmed such that dermal permeability is increased at one or more specific times, permeability is increased for a specific period of time, and so on.

In one embodiment, the energisation signal packet repeats
30 at a frequency of between 1Hz and 100Hz, more particularly between 10Hz and 50Hz.

In one arrangement, each energisation signal packet includes between 12 and 20 energisation signal pulses.

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In one arrangement, the duration of each energisation signal pulse is between 1 μ s and 1s, more particularly between 25 μ s and 100ms.

- 5 The apparatus may take the form of a generally flat member having the means for producing an electromagnetic field and the control means embedded therein.

10 In one arrangement, the therapeutic substance is disposed on a surface of the apparatus. The therapeutic substance may be a drug, vaccine, ion, macromolecule, DNA fragment, gene or any other substance desired to be passed through the skin of a patient for the purpose of obtaining a beneficial effect.

15 In accordance with an alternative aspect of the present invention, there is provided a method of transdermally delivering therapeutic substances, said method comprising:
producing an electromagnetic field;
20 directing the electromagnetic field at a desired treatment area of a patient's skin; and
controlling the electromagnetic field so as to alternately produce active and substantially inactive electromagnetic field portions, each said active
25 electromagnetic field portion including an electromagnetic field packet having a plurality of successive electromagnetic field pulses, and each said substantially inactive electromagnetic field portion including no electromagnetic field pulses.

30 Brief Description of the Drawings

The present invention will now be described, by way of example only, with reference to the accompanying drawings,
35 in which:

Figure 1 is a diagrammatic perspective view of a portion of a stratum corneum prior to application of an

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electromagnetic field produced in accordance with an apparatus and method according to the present invention;

Figure 2 is a diagrammatic perspective view of the stratum corneum shown in Figure 1 during application of an electromagnetic field produced by an apparatus and method in accordance with an embodiment of the present invention;

Figure 3 is a schematic diagram of an energisation signal used to effect energisation of an electromagnetic field generation device of an apparatus in accordance with an embodiment of the present invention;

Figure 4 is an enlarged schematic diagram of an energisation signal packet of the energisation signal shown in Figure 3;

Figure 5 is a schematic diagram illustrating circuitry of an apparatus for facilitating transdermal delivery of therapeutic substances in accordance with an embodiment of the present invention; and

Figure 6 is a diagrammatic perspective view of an apparatus for facilitating transdermal delivery of therapeutic substances in accordance with an embodiment of the present invention, the apparatus including the circuitry shown in Figure 5.

Description of an Embodiment of the Invention

Referring to the drawings, in Figure 1 a portion of a stratum corneum lipid bilayer structure 10 is shown diagrammatically, the lipid bilayer structure 10 having an oily core portion 12 formed of aligned hydrocarbon chains, and charged head portions 14.

During normal conditions, the bilayer structure 10 serves to prevent particles having a size greater than approximately 1nm from passing through.

The inventor of the present invention has discovered that by applying a relatively low power electromagnetic field

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of particular pattern to the stratum corneum, it is possible to cause at least some of the lipids to compact in such a way as to create a void or a region of low lipid population in the stratum corneum through which

5 therapeutic substances may pass. In the present example, the electromagnetic field of predetermined pattern causes a void 16 or region of low lipid population which may be annular to be defined in the stratum corneum as shown diagrammatically in Figure 2, the annular void 16 being
10 temporarily present during and after application of the electromagnetic field, and the structure of the stratum corneum reverting back to the barrier structure shown in Figure 1 at a period of time after cessation of the electromagnetic field.

15 The inventor of the present invention has discovered that by applying an energisation signal 18 of the general pattern shown in Figure 3 to control circuitry of an electromagnetic field generation device such as a coil,
20 the desired effect of creating a temporary aperture in the stratum corneum is achieved. The energisation signal 18 has a general pattern which comprises alternating active and inactive signal portions, the active signal portions containing a plurality of voltage pulses and the inactive
25 signal portions containing no voltage pulses.

In particular, the energisation signal 18 may include an active signal portion in the form of an energisation signal packet 20 which repeats at a frequency of between
30 1Hz and 100Hz, more particularly between 10Hz and 50Hz, with each energisation signal packet including between 12 and 20 successive energisation signal pulses 22, and each successive pair of energisation signal packets 20 being separated by an inactive signal portion 21. The
35 energisation pulses 22 are shown more particularly in an enlarged view of the energisation signal packet 20 shown in Figure 4. The duration of each energisation pulse 22

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may be of the order of $1\mu\text{s}$ to 1s , more particularly $25\mu\text{s}$ to 100ms .

5 In the present example, the time duration of the inactive portion 21, that is the time between successive active portions 20, is greater than the time duration of an active portion 20.

10 In the present example, the duration of each energisation signal pulse 22 is approximately $360\mu\text{s}$, the duty cycle of each of the energisation signal pulses 22 is approximately 50%, and the time duration of each inactive signal portion 21 is 15 times greater than the time duration of each active signal portion 20, although it will be understood
15 that other variations are possible. Each energisation signal pulse 22 in the present example is of generally rectangular shape.

20 It will be understood that by applying energisation signal pulses 22 of generally rectangular shape to control circuitry of an electromagnetic field generation device such as a coil, active electromagnetic field portions separated by inactive electromagnetic field portions are produced, with each active electromagnetic field portion
25 containing packets of electromagnetic field pulses produced at a spacing determined by the duration of an inactive electromagnetic field portion, and each inactive electromagnetic field portion containing no electromagnetic field pulses. In the present example, the
30 electromagnetic field strength of the electromagnetic field signal is of the order of 3 Gauss or less.

Without wishing to be bound by theory, it is believed that permeability of the stratum corneum is enhanced by
35 application of an electromagnetic signal of the type produced when an energisation signal of the general pattern shown in Figure 3 is applied to control circuitry

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of an electromagnetic field generation device, because the plurality of electromagnetic pulses in the active field portion cause charging of portions of the bilayer structure and thereby creation of a potential difference in the structure, and the inactive field portions cause the accumulated charge to dissipate across the lipid bilayer. This causes portions of the bilayer structure to repel each other and thereby form an opening in the stratum corneum through which therapeutic substances may pass. In other words, it is believed that the electromagnetic field does not in itself have any biological effect on the stratum corneum, rather the electromagnetic field induces an electrical or ionic effect in the stratum corneum which causes gaps to occur in the stratum corneum. In view of this, it is believed that the amount of charge generated in the bilayer structure and thereby the degree of permeability is dependent in particular on the number of pulse edges of the energisation signal per unit time, the total number of pulse edges, and the packet frequency.

The inventor of the present invention has also discovered that the present transdermal delivery technique makes it possible to accurately target within 3 dimensions a desired treatment area by locating the electromagnetic field generation device (in this example a coil) above the desired treatment area, and modifying the packet frequency so as to influence the stratum corneum bilayers with little or no detectable effect in surrounding tissue.

Referring to Figure 5, circuitry 24 is shown for effecting generation of an electromagnetic signal having a pattern suitable for causing an aperture to be produced in a stratum corneum.

The circuitry 24 includes a solid state switching device, in this example in the form of a bipolar transistor 26

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connected in series with an electromagnetic field generation device, in this example in the form of a coil 28. Switching of the transistor 26 and thereby energisation of the coil 28 is controlled using control circuitry, in this example in the form of a microcontroller 34 preprogrammed to generate a biasing signal on the base of the transistor 26 corresponding in general pattern to the energisation signal 18 shown in Figure 3. However, it will be understood that other arrangements for effecting controlled switching of the transistor 26 are envisaged.

In this example, a voltage regulator 36 is also provided to produce a regulated voltage necessary for the microcontroller 34, although it will be understood that for microcontrollers or other control circuitry which do not require a regulated voltage supply, the regulator 36 may be omitted.

As shown in Figure 6, an apparatus 40 for facilitating transdermal delivery of therapeutic substances may take the form of a generally flat rectangular member which for example may be formed of plastics material. The apparatus 40 includes a body portion 42 having embedded circuitry 24 and an energy storage device such as a battery 44 for supplying power to the circuitry 24. However, it will be understood that other types of apparatus may be used, and that the apparatus may be mains powered.

During use, the apparatus 40 may be placed adjacent a portion of the skin through which it is desired to introduce therapeutic substances and the circuitry 24 activated so as to cause opening of an aperture in the stratum corneum adjacent the apparatus 40.

The therapeutic substance may be disposed on a surface 46 of the body portion 42, may be applied directly to the

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skin, or may be introduced on to the skin in any other suitable way.

In an experimental example, penetration of caffeine
5 through excised human epidermal membranes was investigated using Franz-type diffusion cells and standard procedures. An electromagnetic field pattern was created and the penetration results compared with passive diffusion. The
10 electromagnetic field pattern used was generated by applying an energisation signal having 12 pulses at a repeating frequency of 10Hz to a coil. Each of the pulses has a duration of approximately 360 μ s. A phosphate buffered saline receptor solution was used and the amount of caffeine in the receptor solution determined by HPLC
15 with UV detection at regular time intervals up to 6 hours post application of the electromagnetic field. In this example, the electromagnetic field pattern was applied for approximately 30 minutes.

20 It was observed that the caffeine flux associated with passive diffusion was of the order of 4.1 $\mu\text{gcm}^{-2}\text{h}^{-1}$. It was also observed that the caffeine flux associated with the electromagnetic field patterns of the present invention were significantly higher than the corresponding caffeine
25 flux associated with passive diffusion, with the highest caffeine flux achieved being 19.24 $\mu\text{gcm}^{-2}\text{h}^{-1}$.

Similar experiments were carried out with electromagnetic fields generated by applying an energisation signal having
30 15 pulses of 360 μ s duration at a repeating frequency of 20Hz to a coil, and by applying an energisation signal having 255 pulses at a repeating frequency of 2Hz to a coil. These experiments yielded caffeine flux values of 7.20 $\mu\text{gcm}^{-2}\text{h}^{-1}$ and 8.51 $\mu\text{gcm}^{-2}\text{h}^{-1}$, although the latter of
35 these experiments produced an effect only after 60 minutes.

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A further experiment was carried out by applying an energisation signal having a single quasi-rectangular pulse repeated at 72Hz to a coil. This yielded no discernable change in permeability of the stratum corneum.

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It will be appreciated that although the present embodiment is described in relation to common rail mode generation of an electromagnetic signal, other arrangements are possible, such as biphasic mode generation of an electromagnetic signal.

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It will be appreciated that the amount of energy required to carry out the present transdermal delivery technique is approximately 1000 times less than the corresponding energy levels required for iontophoresis and electroporation transdermal delivery techniques. As a consequence, the present technique is ideally suited to implementation in compact, portable and disposable applications, in particular for outpatient and homecare use.

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It will also be appreciated that since the present technique is inductive, the technique can operate through most non-conductive materials such as bandages without the requirement for physical contact with the skin.

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It will also be appreciated that the present technique can not be sensed or felt by humans and, as a result, the technique is painless and has none of the undesirable side effects commonly associated with techniques such as iontophoresis and electroporation.

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It will also be appreciated that the control circuitry, for example a microcontroller, may be configured so that the apparatus carries out a specific treatment plan, for example by generating an appropriate energisation signal pattern and using the energisation signal to apply one or

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more specific electromagnetic field patterns to a target area of a patient at specific times of for a specific time duration.

- 5 It will also be appreciated that the therapeutic substance may be a drug, vaccine, ion, macromolecule, DNA fragment, gene or any other substance desired to be passed through the skin of a patient for the purpose of obtaining a beneficial effect.

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Modifications and variations as would be apparent to a skilled addressee are deemed to be within the scope of the present invention.